and transfer learning

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Experiments and results

White matter hyperintensities (WMH)

WMH:

- are a manifestation of small vessel diseases.
- can be everywhere in white matter,
- play a key role in stroke, demantia and ageing.

Importance of WMH study:

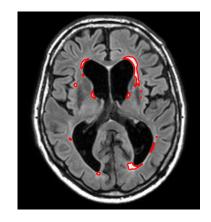
- analysis (shape, volume, location) is needed for clinical research studies.
- associated with clinical symptoms, can help prognosis, diagnosis, treatment monitoring etc.

Problem: manual segmentation is time-consuming and observer-dependent.

Challenge MICCAI

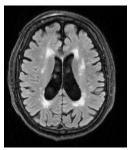
- Segmentation of WMH
- Part of Brain Lesion (BrainLes) MICCAI 2017 Workshop
- Method submitted in a Docker container

Test data was not released

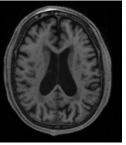


http://wmh.isi.uu.nl/

Data



(a) FLAIR image



(b) T1 image



(c) Ground Truth

Origin of the datasets

Context

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Institute	Scanner	Train	Test
UMC Utrecht	3T Philips Achieva	20	30
NUHS Singapore	3T Siemens TrioTim	20	30
VU Amsterdam (AMS)	3T GE Signa HDxt	20	30
	1.5T GE Signa HDxt	0	10
	3T Philips Ingenuity	0	10

Each volume is composed of about 45 slices used to generate the 2D input images for the network.

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Experiments and results

Previous work

Our WMH segmentation is inspired by our previous work¹ on brain segmentation.

Reminder: VGG is a network:

- pretrained on ImageNet (database of hundreds of color natural images),
- dedicated to visual object detection in 2D color images,
- including a base network.

¹Y. Xu *et al.* From neonatal to adult brain MR image segmentation in a few seconds using 3D-like fully convolutional network and transfer learning. In Proc. of IEEE Intl. Conf. on Image Processing (ICIP), pp. 4417–4421, Beijing, China, Sep 2017.

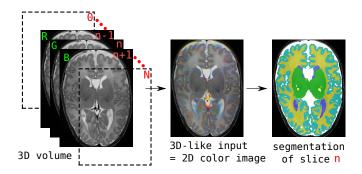
Previous work

A segmentation method based on VGG-16:

- Preprocessing: preparation of a set of 2D RGB images from a 3D volume pseudo-3D approach
- Learning: transfer learning and modification of VGG-16 network
- Results: inference on 2D color images, and reconstruction of 3D images

Key idea: A 2D color image encodes also 3D information.

For each slice n do



First experiment:

Use of the pseudo-3D approach with VGG-16 on WMH data.

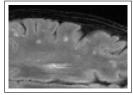
Observation:

The network fails to detect small lesions.

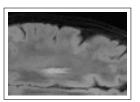
Idea:

Help the network by enhancing these small lesions in the input data.

$$top-hat(I) = I - \gamma(I),$$
 where $\gamma(I)$ is the morphological area opening of I .



FLAIR



opening of FLAIR

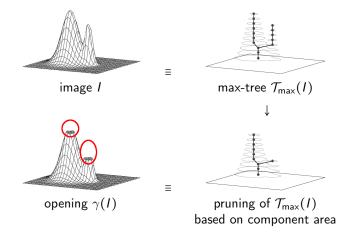


top-hat

We apply this procedure for each slice of a FLAIR volume.

A morphological preprocessing

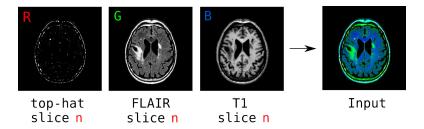
Method



The top-hat is the **residue** (difference) between I and $\gamma(I)$.

Preprocessing: from 3D volumes to 2D images

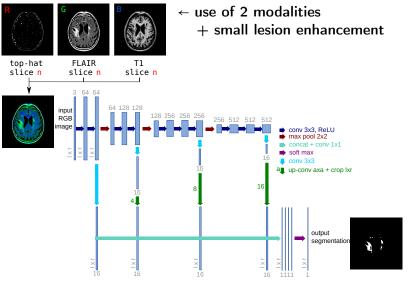
For each slice n, do:



2 gray 3D volumes (FLAIR + T1) + 1 generated (top-hat) → a set of RGB 2D images

(It is not pseudo-3D anymore: each input 2D color image comes only from one slice.)

Network



Parameters.

- Total number of iterations: 150k
- Learning rate: 10^{-8} for the first 50k iterations

 10^{-10} for the last 100k

Momentum:

0.99 for the first 50k iterations 0.999 for the next 100k

- Weight decay: 0.0005
- 4 stages only

Experiments and results

- Experiments and results

- 30 patients for training/30 patients for testing (10 from each hospital).
- Augmentation of training data (with scale variations and rotations).
- Input images:
 a series (3D volume) of 2D color images.

Training phase: for the challenge

- Model trained on all the 60 "expanded" patients.
- For each patient in the test dataset: pre-processing, centering, inference and reconstruction are fully automated
- Runtime on a 3D volume is less than 10 seconds on average.

Evaluation

Dice: Dice coefficient

H95: Hausdorff distance (modified, 95th percentile)

AVD: Average volume difference

Recall: Sensitivity for individual lesions

F1: F1 =
$$2PR/(P+R)$$
,

where P and R are respectively the precision and recall for individual lesions:

P = true positives / (trues positives + false positives)

R = true positives / (trues positives + false negatives)

Туре	Dice ↑	AVD ↓	Recall ↑	F 1 ↑
pseudo-3D	0.72	23.90	0.38	0.46
2D without top-hat	0.72	28.24	0.39	0.48
2D with top-hat	0.75	22.63	0.61	0.63

 \uparrow means the higher the better / \downarrow means the lower the better

Two conclusions:

- Pseudo-3D is useless here.
- Adding a morphological pre-processing gives much better results.

Quantitative results

Results of our method on the challenge dataset:

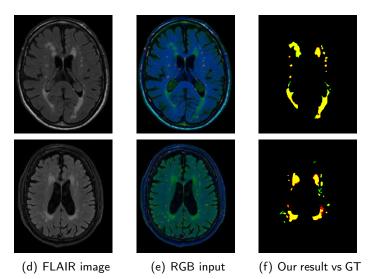
Experiments and results

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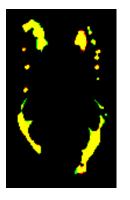
Origin	Dice ↑	H95 ↓	AVD↓	Recall ↑	F1 ↑
UMC Utrecht	0.74	11.22	19.07	0.70	0.66
NUHS Singapore	0.77	8.28	17.64	0.61	0.68
AMS GE 3T	0.75	6.75	21.91	0.62	0.71
AMS GE 1.5T	0.73	10.94	16.66	0.60	0.71
AMS Philips 3T	0.50	70.27	46.33	0.57	0.53
Weighted average	0.73	14.54	21.71	0.63	0.67

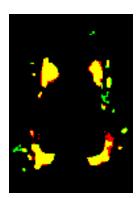
6th place of the challenge (among 21 competitors). Rank:

Some qualitative results



Some qualitative results: zoomed in





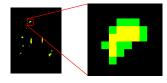
Yellow: true positives; Red: false positives; Green: false negatives

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- Fast, robust and automated method for WMH segmentation:
 - inspired from our pseudo-3D approach (ICIP'17)
 - transfer learning works for some med. image segmentation tasks
- Segmentation of a 3D volume in less than 10 seconds:
 - Benefits from merging modalities in a color image...
 - ...and using a simple 2D network
- Effective benefits of morphological preprocessing:
 - highly non-linear
 - helps the network to identify objects of interest
- Docker container downloadable on our website:
 - reproducible research is important...

Perspectives

• Improvement possible thanks to post-processing?



Application to other segmentations, pathological or not

 Going further with predictions? (prediction of tumor proliferation score for breast cancer, prediction of patient overall survival from the study of brain lesions, etc.)

The end

Supplementary materials and Docker file:

https://www.lrde.epita.fr/wiki/NeoBrainSeg



Thanks for your attention! Any questions?

Results of the methods of the challenge

Sorted by increasing AVD:

Team	Dice ↑	H95 ↓	AVD ↓	Rec ↑	F1 ↑
nlp_logix	0.77	7.16	18.37	0.73	0.78
k2	0.77	9.79	19.08	0.59	0.70
ipmi-bern	0.69	9.72	19.92	0.44	0.57
misp	0.72	14.88	21.36	0.63	0.68
LRDE	0.73	14.54	21.71	0.63	0.67
 median 	0.68	14.55	34.34	0.58	0.52